The Fabrication of the Microfluidic Device with Micro- and Nano- Scale Channels

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Abstract — Here a simple method for fabrication of the microfluidic device with micro- and nanochannels was developed. The microchannels in micro and nano scales were fabricated on a glass substrate during a two- step process respectively. And then the glass substrate with the microchannels was bonded with another flat glass substrate at room temperature to avoid the collapse of the nanochannels. Standard UV lithography and wet etching were used in this method. The nanochannels with a series of depths were obtained with optimized etchant concentration of $1.5 \times 10^{-2}$ mol L$^{-1}$ HF, $7.5 \times 10^{-3}$ mol L$^{-1}$ HNO$_3$, and $7.5 \times 10^{-3}$ mol L$^{-1}$ NH$_4$F, and the depth had a linear relationship with the etching time (the square of correlation coefficient was 0.9983). The roughness length of the etched nanochannel was 2.045 nm investigated by atomic force microscopy (AFM). The substrate was then bonded with a flat glass plate to form a closed microchannel, the cross-section of the bonded microchannel was imaged by a scanning electron microscopy (SEM). With this method, the microchannels combined with micro and nano scale can be prepared conveniently with low cost.

Keywords— microfluidic device; nanochannel

I. INTRODUCTION

Microfluidic devices have been proved a powerful tool and applied in many fields. With the shortened diffusion distance, the microfluidic device can realize fast and sensitive analysis with decreased consumption. When the dimension of the microchannel decreased into nanometer scale, the unique properties emerged such as overlapped electric double layer, increased surface tension, influence of the solid surface and quantum effect, which are very attractive for fundamental research. Because of the further decreased diffusion distance and confine space for nanoparticle and single molecule, the microfluidic device with nanochannel can be utilized in a wide range of applications, such as biomolecule analysis [1], detection [2].

The nanochannels were at least one of the dimensions smaller than 100 nm [3]. Many methods had been developed to fabricate the nanochannels; such as electron-beam lithography (EBL) [4], focused-ion beam (FIB) [5], proton beam writing (PBW) [6]. These methods realized the nanochannels with the precise control, but they were cost expensive and difficult to scale up. Surface nanomachining [7] was also used to fabricate the nanochannels by removing the sacrificial layer from the integrated device, but it also needed tens of hours of etching. Nanoimprint lithography [8] can only be used to fabricate the device with simply design. Buried channel technology [9] was very complex and chemical vapor deposition (CVD) was needed. All these methods did not satisfy the demand of the development of nanofluidic device. He [10] reported a method to fabricate the glass device by wet etching and room temperature bonding. The microchannels and nanochannels were etched in two glass substrates and then bonded together. During bonding, the two glass substrates needed to be aligned very precisely, and was not suitable for mass production. Here the microchannels and nanochannels were fabricated in the same glass substrate by two steps exposure, and then bonded to realized the final microfluidic device. By this method, the microfluidic device with microchannels and nanochannels can be prepared with simple, low cost and reliable characters.

II. EXPERIMENT

The fabrication of glass microfluidic device with the microchannels and nanochannels was according to the standard photolithographic and wet chemical etching protocol. A method with two steps was developed, one step for the fabrication of the microchannels, and the other for the nanochannels. The process was described briefly as the fig. 1 shown.

A SG2506 glass substrate with chromium and AZ1805 photore sist coating (Shaoguang Microelectronics Co., Changsha, China) was exposed through a photo mask by a MA6/BA6 mask aligner (SÜSS MicroTec AG, Garching, Germany). The photo mask was designed with the pattern of
the microchannels, and the design was transferred onto the
glass substrate. Then the microchannels were etched by 1 mol
L⁻¹ HF and 1 mol L⁻¹ NH₄F at 40 °C. The microchannels with
the depth of 25 μm were achieved after 20 min etching.

Fig. 1 Schematic diagram of the fabrication of the microfluidic device with
microchannels and nanochannels.

The glass substrate with the microchannels was spun and
coated by another photoresist (BP212), and a second UV
exposure was carried out through another photo mask. On this
photo mask, the pattern of the nanochannels was designed.
Then the glass substrate was etched in diluted etchant
(1.5×10⁻² mol L⁻¹ HF, 7.5×10⁻³ mol L⁻¹ HNO₃ and 7.5×10⁻³
mol L⁻¹ NH₄F) at 40 °C. The depth of nanochannels was
controlled by adjusting the etching time.

The access holes were drilled on the etched substrate at the
ends of the microchannels and nanochannels. Then room
temperature bonding was carried out to bond the etched
substrate with a flat glass substrate, and then the closed
channels were formed. The microfluidic chip was ready for
use after aging for 3~7 days.

III. RESULT AND DISCUSSION

The etching of nanochannel was critical important for the
whole process. Usually the microchannels were etched in the
solution with high concentration, the etching rate was around
2.5 μm min⁻¹. The etching time would be several seconds, and
it was very difficult to realize the precise control over the
nanochannel’s depth. According to the report [10], the etchant
with dilute concentration was adopted, and the etching time
would increased into tens of minutes. As fig. 2 shown, the
etching time was optimized and found to be linear with the
channel’s depth. The etching time was increased from 5 min
to 30 min, the nanochannel’s depth also increased from 35.2
nm to 242.3 nm. The square of correlation coefficient was
0.9983, the etching rate was calculated to be 7.65 nm min⁻¹.
For each point in fig.2, the nanochannel’s depth was measured
by surface profiler at three different positions. The standard
deviations in the fig. 2 proved that etching was very uniform
for the whole glass substrate.

Fig. 2 The etching depth varied with the etching time. Etchant: 1.5×10⁻² mol
L⁻¹ HF, 7.5×10⁻³ mol L⁻¹ HNO₃ and 7.5×10⁻³ mol L⁻¹ NH₄F. Etching
temperature was 40 °C.

Fig. 3 The effect of etchant concentration on the depths of nanochannel.
Molar concentration ratio of HF- HNO₃- NH₄F was 1:0.5:0.5, etching for 10
min at 40°C.

The etchant’s concentration had obvious influence on the
channel’s depth, and the etchant with two different
concentrations was compared. The first etchant had $1.5 \times 10^{-2}$ mol L$^{-1}$ HF, $7.5 \times 10^{-3}$ mol L$^{-1}$ HNO$_3$ and $7.5 \times 10^{-3}$ mol L$^{-1}$ NH$_4$F (molar concentration ratio of HF: HNO$_3$: NH$_4$F = 1: 0.5: 0.5), the second etchant’s concentration was ten times higher (the molar concentration ratio was kept the same). After 10 min’s etching, the etching depth for the first etchant was 70.4±3.0 nm, while the etching depth for the second one was 2497±66.5 nm, which the result was shown in fig. 3. The calculated etching rate was 250 nm min$^{-1}$, which was around 36 times more than the first etchant’s.

Because high etching temperature would decrease the etchant’s concentration for HF’s volatility. 40°C was chosen as the etching temperature to avoid the HF from volatilizing and keep the concentration constant.

By adjusting the etching time, the nanochannel with depths ranging from tens of nanometers to several hundreds nanometers can be realized. As shown in fig. 4, the average depth was 91.9 nm after 13 min etching. The roughness lengths before and after etching were 3.5 nm and 2.8 nm respectively. The etching did not increase the surface roughness of the glass substrate obviously. The depth of the nanochannel can also be confirmed by the SEM image of its cross section. In fig. 5, the microfluidic device was cut and scanned by SEM. The dark area in the middle was the nanochannel, whiles the gray areas above and below the nanochannel were the glass substrate. The depth of the nanochannel was 105 nm. The top and bottom walls were also very smooth.

Fig. 6 was the AFM image of the bottom and edge of nanochannel. The average roughness length of the etched nanochannel was 2.045 nm, and the sharp peaks in fig 6a were the nanoparticle and nanofibers on the surface of nanochannel. The fig. 5b showed the edge of the nanochannel. The roughness of the edge was produced by the photo mask and photolithography.

IV. CONCLUSION

Here we demonstrated a low cost and easy manipulated method for the fabrication of nanofluidic channels on glass substrates. With this method, a combined microchannels and nanochannels device was successfully fabricated. This technique can be used for the preparation of nanofluidic devices for the applications of chemical analysis, clinical diagnostic and many other purposes.

REFERENCES


